

OCT phantoms with known attenuation

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Tissue mimicking phantoms

[introduction](#)

OCT signal

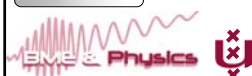
Phantoms:

silicone

liquid

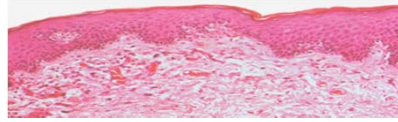
conclusion

- Morphology
- Scattering (and absorption)
- Understanding *in vivo* measurements
 - OCT signal
 - Scattering properties of phantoms
 - Retinal phantom test

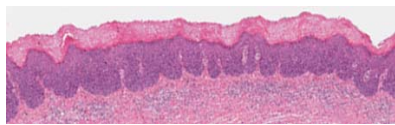
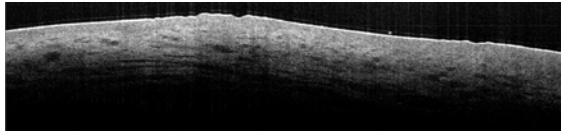


Skin: histology and OCT images

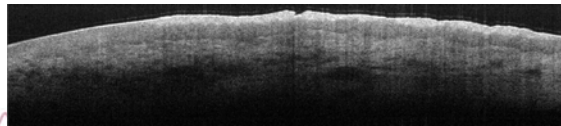
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healthy epidermis
 mean 0.5 mm
Wilkinson. Atlas of Vulvar Disease 2008



VIN epidermis
 0.35- 1.66 mm, mean
0.93 ± 0.37mm



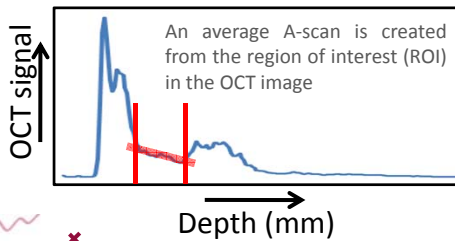
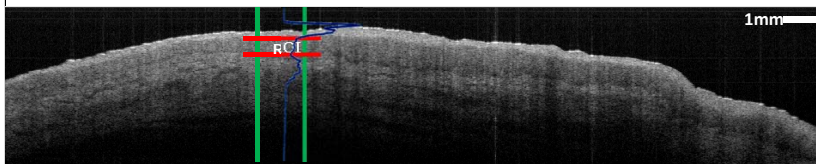
Baggish. Obstet Gynecol 1989



Fitting procedure

- [introduction](#)
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The OCT signal decreases with depth
 Depends on scattering of the sample



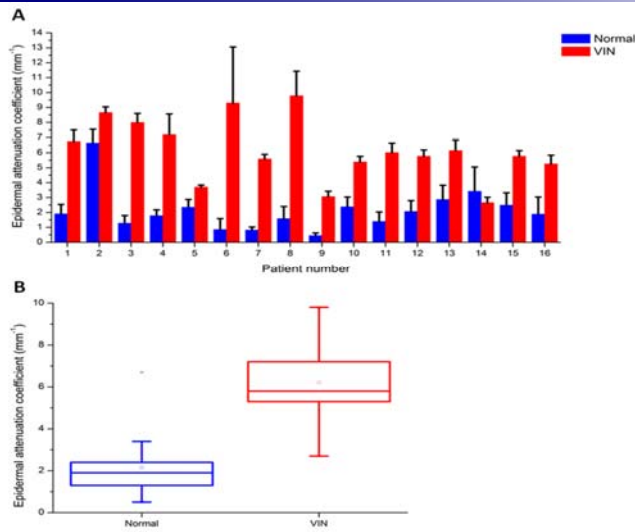
$$i_d \propto \left[e^{-2\mu_{\text{OCT}}z} \right]^{\frac{1}{2}}$$

The **data** of the tissue part that is of interest can be fitted with single scattering model



Quantitative analysis of OCT signals: μ_t

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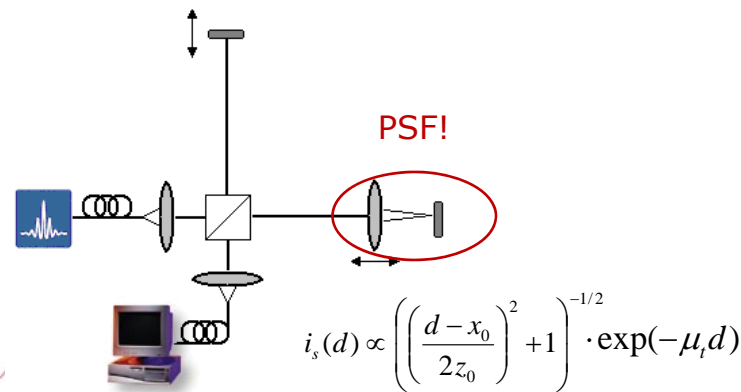


Cauberg et al, JBO 2010, ex-vivo Bladder cancer
Barwari et al, Journ of EndoUro, 2011, ex-vivo kidney tumor
Barwari et al, BJU int, 2012, in-vivo kidney tumor
Wessels et al, JBO 2012, in-vivo vulvar neoplasia
Bus et al, J Urol 2013, in vivo ureters

Optical Coherence Tomography (OCT)

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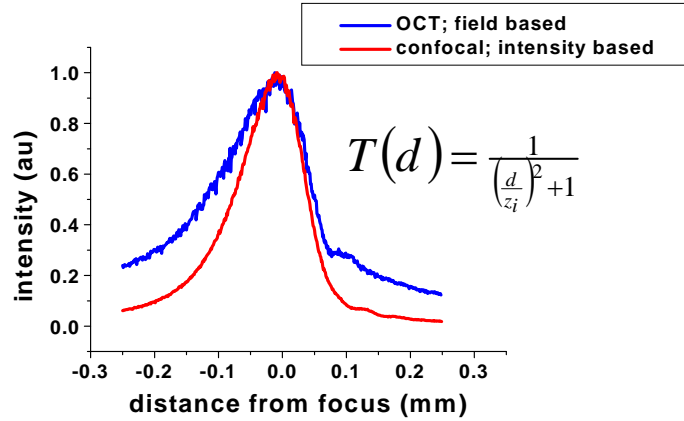
- Path length is known
- Can we measure μ_s by OCT signal analysis?
- Theory:
 - Single scattering model
 - OCT = extension of confocal microscope



confocal layout

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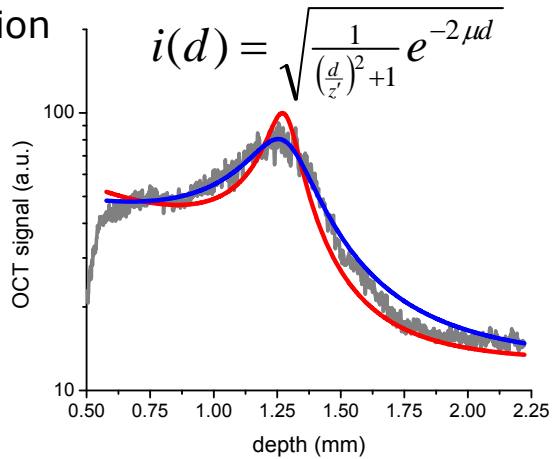
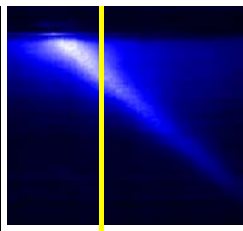
Transfer function mirror reflection



retrieving μ_t

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vertical section



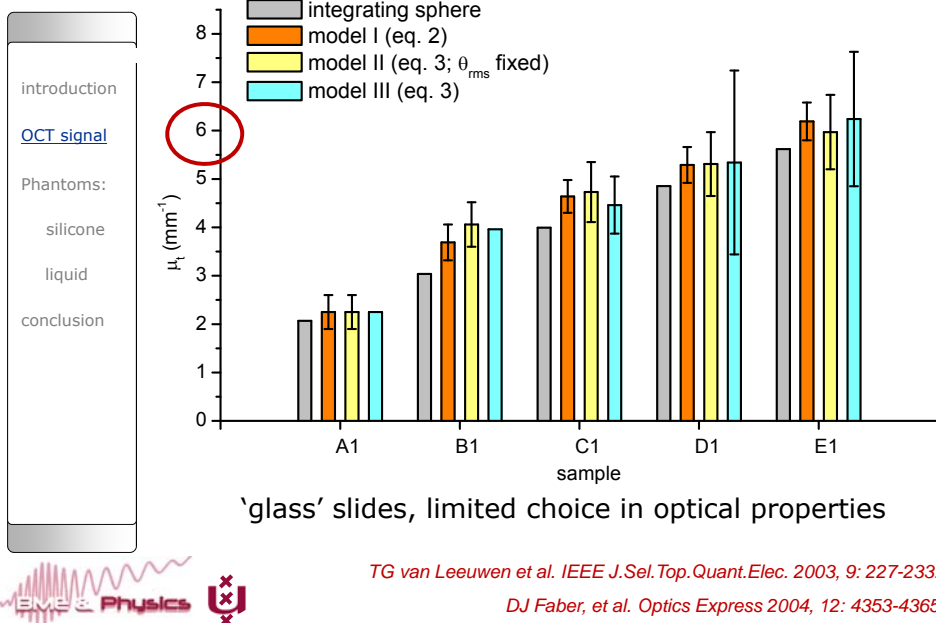
$z' = 63 \mu\text{m}; \quad \mu = 2.3 \pm 0.6 \text{ mm}^{-1}$

$z' = 126 \mu\text{m}; \quad \mu = 1.6 \pm 0.3 \text{ mm}^{-1}$



dirk faber/

calibrated samples from Lund



Journal of Biomedical Optics 15(2), 025001 (March/April 2010)

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Optical phantoms of varying geometry based on thin building blocks with controlled optical properties

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Abstract. Current innovations in optical imaging, measurement techniques, and data analysis algorithms express the need for reliable testing and comparison methods. We present the design and characterization of silicone elastomer-based optical phantoms. Absorption is included by adding a green dye and scattering by adding TiO₂ or SiO₂ particles. Optical coherence tomography measurements demonstrate a linear dependence of the attenuation coefficient with scatterer concentration in the absence of absorbers. Optical transmission spectroscopy of the nonscattering absorbing phantoms shows a linear concentration dependent absorption coefficient. Both types of samples are stable over a period of 6 months. Confocal microscopy of the samples demonstrates a homogeneous distribution of the scatterers, albeit with some clustering. Based on layers with thicknesses as small as 50 μm, we make multilayered structures resembling flow channels, (wavy) skin-like structures, and a layered and curved phantom resembling the human retina. Finally, we demonstrate the ability to incorporate gold nanoparticles within the phantoms. In conclusion, our phantoms are easy to make, are based on affordable materials, exhibit well-defined and controllable thickness, refractive index, absorption, and scattering coefficients, are homogeneous, and allow the incorporation of novel types of nanoparticle contrast agents. We believe our phantoms fulfill many of the requirements for an "ideal" tissue phantom, and will be particularly suited for novel optical coherence tomography applications. © 2010 Society of Photo-Optical Instrumentation Engineers. [DOI: 10.1117/1.3369003]

Keywords: biomedical optics; imaging systems; optical properties; scattering; absorption.

Paper 09516R received Nov. 19, 2009; revised manuscript received Jan. 22, 2010; accepted for publication Jan. 26, 2010; published online Apr. 12, 2010.

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De Bruin et al. JBO. 2010

Kitchen Hardware

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Glass plates: 15 *
15 * 1 cm



Spacers: ≥ 50
 μm



Tissue
homogenizer



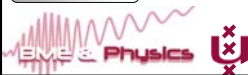
Vacuum pump



Ultrasonic bath



Mixer



De Bruin et al. JBO. 2010

Ingredients 1

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Sylgard ® 184 Silicone Elastomer
DOW/Corning

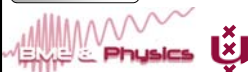


Silicone: 9 parts

Elastomer: 1 part

<http://www.dowcorning.com/>

- Optical 'clear' material
- Thermal conductivity: 0.17 W /mK (soft tissue range)
- Elongation at break : 140%
- Density: 0.97 kg/l



De Bruin et al. JBO. 2010

Ingredients 2

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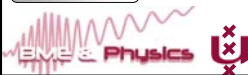
Titanium dioxide (TiO₂)
 Sigma Aldrich
 Refractive index 2.49 (anatase form)
 Mean radius ~50 nm (unknown distribution)

Glass particles (SiO₂)
 Kisker biotech
 Refractive index 1.37
 Mean radius: 500±58 nm

Scattering

Absorber ABS 551
 Exciton

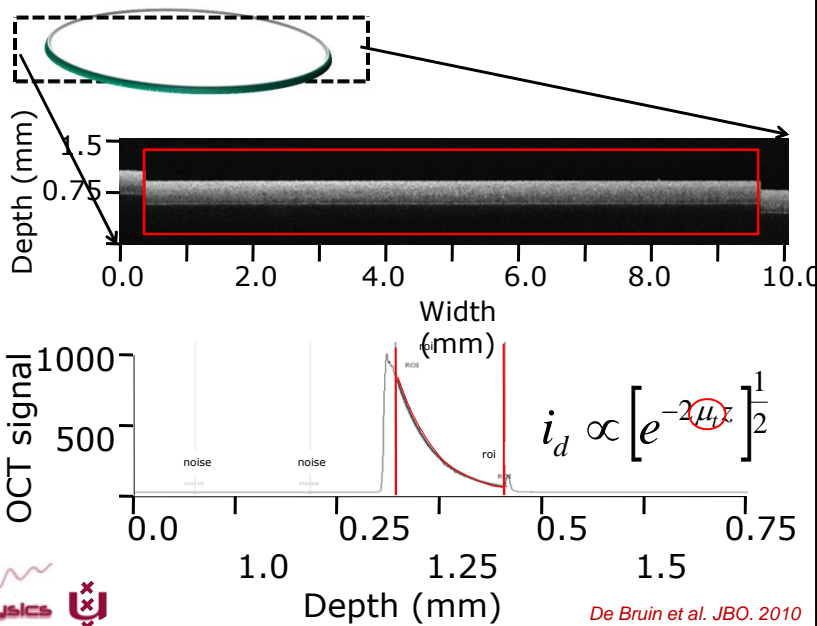
Absorption



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Thin Layered Phantoms

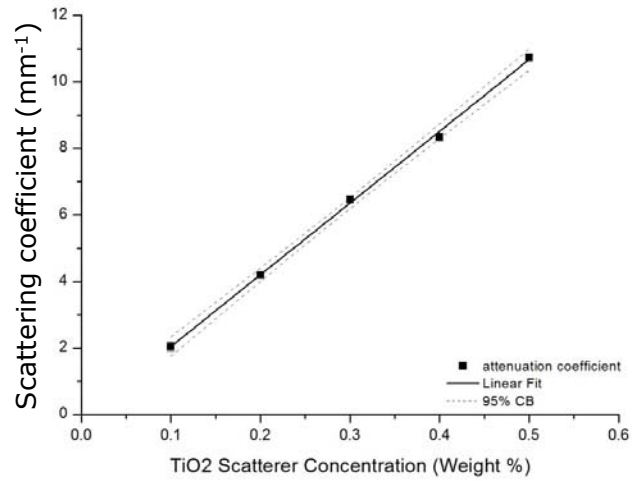
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De Bruin et al. JBO. 2010

Scattering TiO2 (OCT data @ 800 nm)

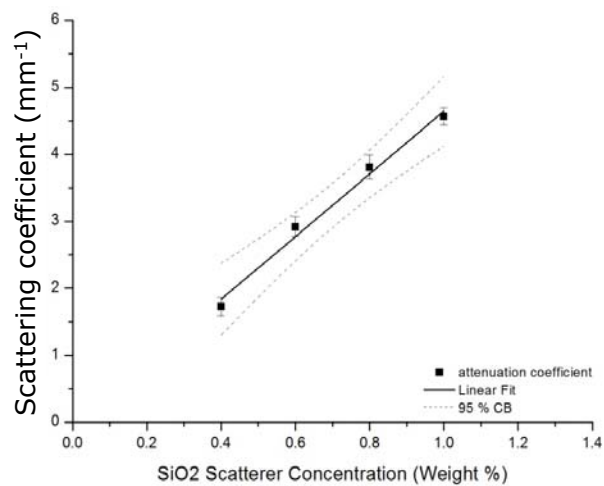
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De Bruin et al. JBO. 2010

Scattering SiO2 (OCT data @ 800 nm)

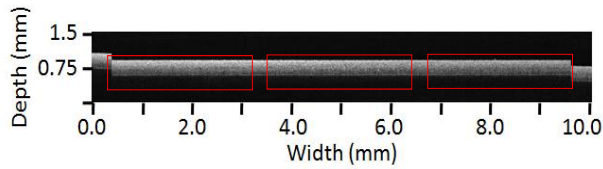
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De Bruin et al. JBO. 2010

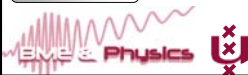
Macroscopic Homogeneity

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OCT at 850 nm

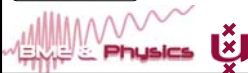
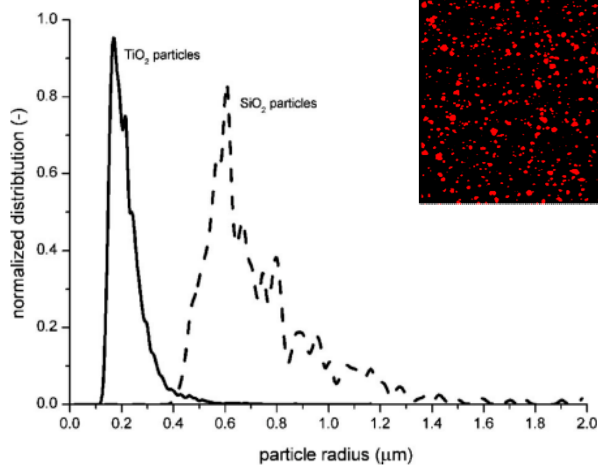
Concentration weight %	μ_t roi1 mm^{-1}	μ_t roi2 mm^{-1}	μ_t roi3 mm^{-1}	Mean $\mu_t \pm \text{SD}$ mm^{-1}	$\Delta \mu_t$ %
0.1	1.75	2.00	1.93	1.89 ± 0.16	8.5
0.2	4.25	5.15	5.17	4.86 ± 0.08	1.6
0.3	7.50	7.64	6.73	7.29 ± 0.21	2.9
0.4	8.21	8.29	8.75	8.42 ± 0.29	3.4
0.5	10.00	11.30	11.6	10.97 ± 0.38	3.4



De Bruin et al. JBO. 2010

Microscopic Homogeneity

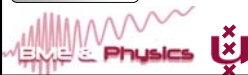
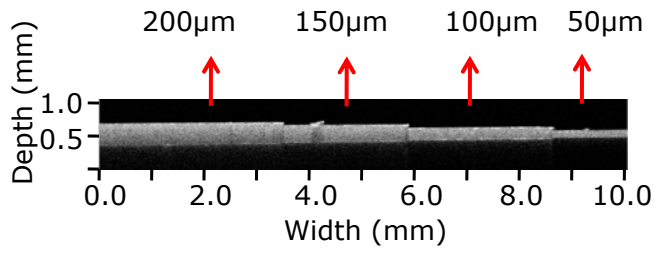
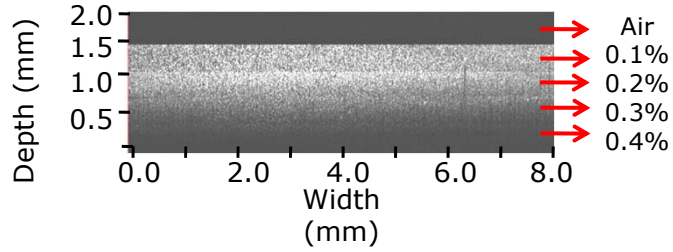
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De Bruin et al. JBO. 2010

Thin Layered Phantom Stack

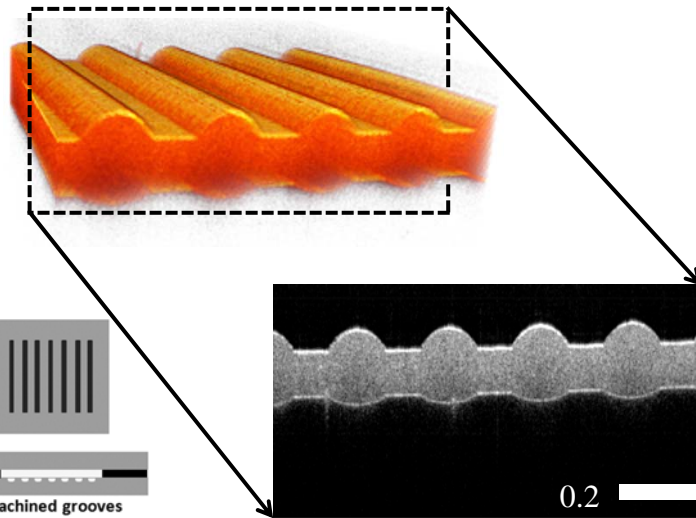
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De Bruin et al. JBO. 2010

Skin simulating phantom

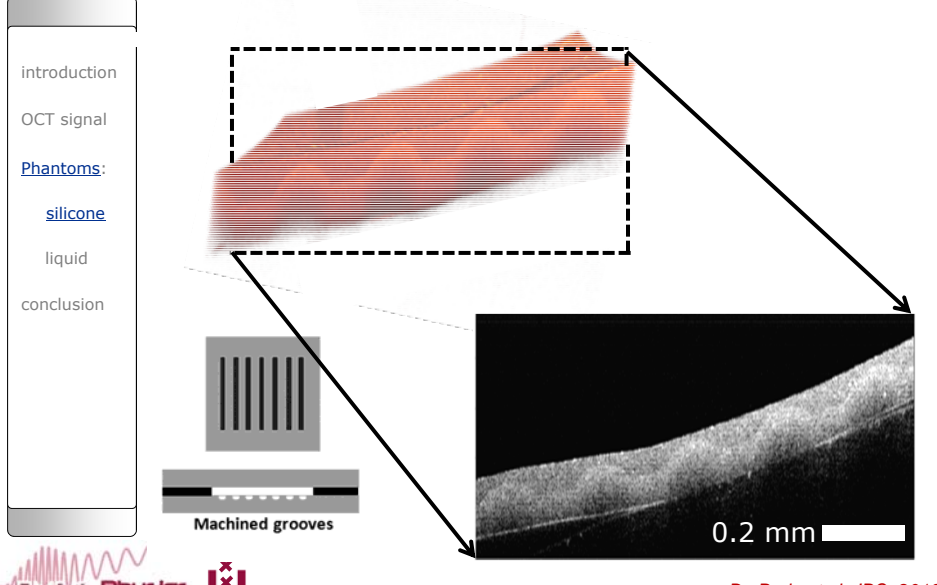
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De Bruin et al. JBO. 2010


Skin simulating phantom

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Machined grooves

0.2 mm

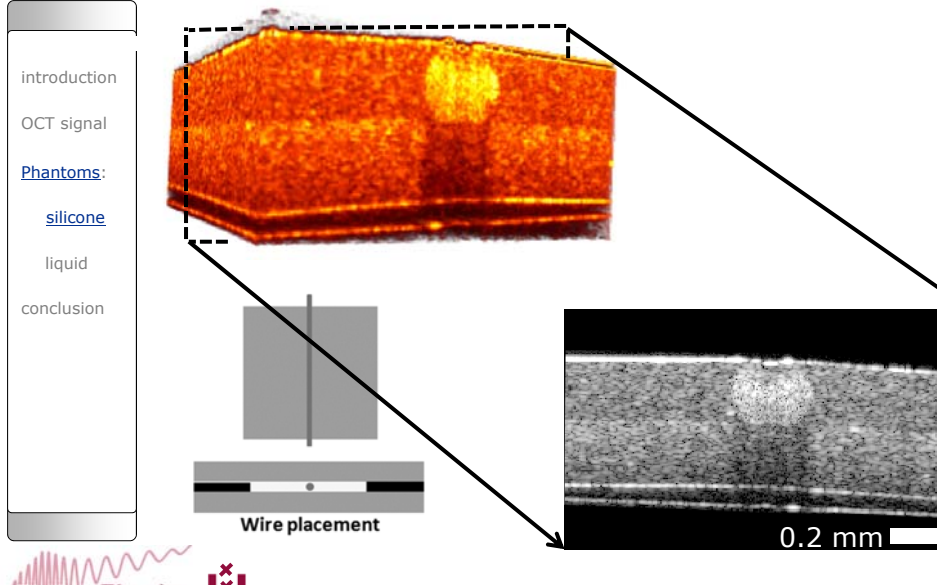
EME & Physics 

De Bruin et al. JBO. 2010

The diagram illustrates the construction of a skin simulating phantom. It shows a 3D perspective view of a rectangular block with a textured surface. A dashed box highlights a section of the block, which is magnified in an OCT image on the right. The OCT image shows a cross-section of the phantom with a scale bar of 0.2 mm. Below the 3D view, a schematic diagram shows a cross-section of the phantom with vertical lines representing 'Machined grooves'.


Vessel Simulating Phantom

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Wire placement

0.2 mm

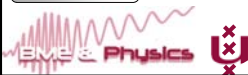
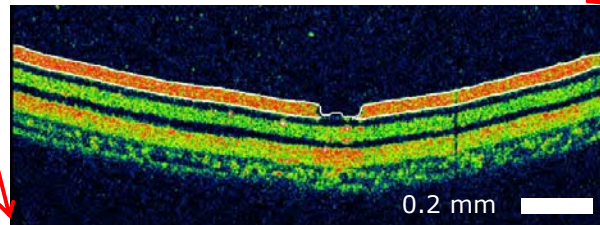
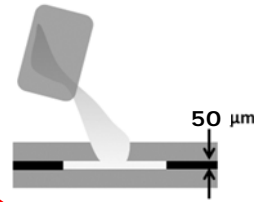
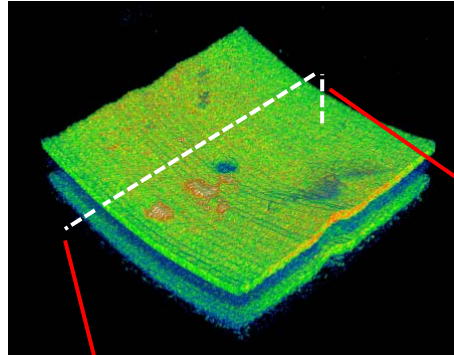
EME & Physics 

De Bruin et al. JBO. 2010

The diagram illustrates the construction of a vessel simulating phantom. It shows a 3D perspective view of a rectangular block with a textured surface. A dashed box highlights a section of the block, which is magnified in an OCT image on the right. The OCT image shows a cross-section of the phantom with a scale bar of 0.2 mm. Below the 3D view, a schematic diagram shows a cross-section of the phantom with a vertical line representing 'Wire placement'.

Retina Simulating Phantom

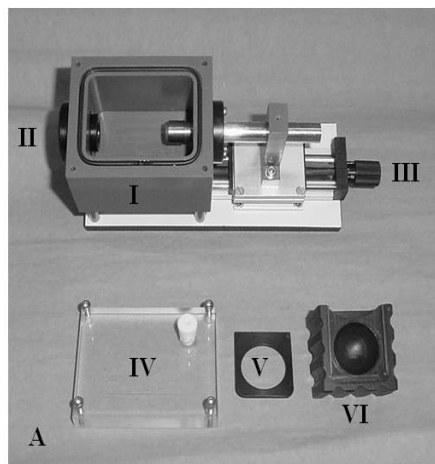
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De Kinkelder et al. J Bio-Photonics 2013

Retina Simulating Phantom

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Comparison of OCT systems

introduction

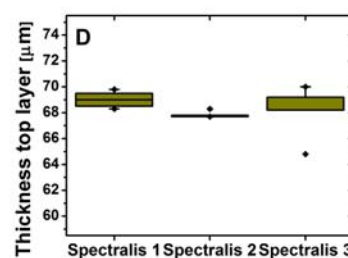
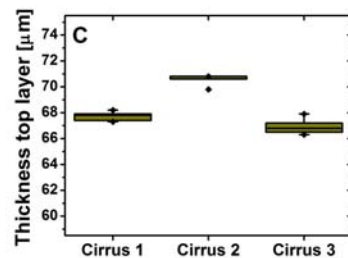
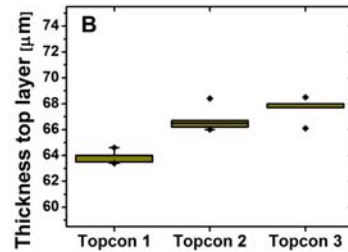
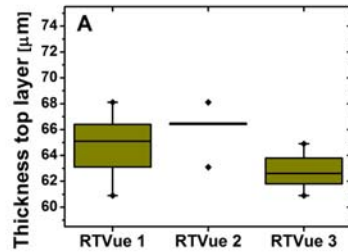
OCT signal

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So...

introduction

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Durable phantoms (~14 % stability in 6 months)

Concentration dependent scattering and absorption (2~11 mm⁻¹)

Tissue comparable index of refraction (1.42 ±0.01)

Advanced 'tissue mimicking' geometry (skin, retina, channels)

Homogeneity (> 8 %)

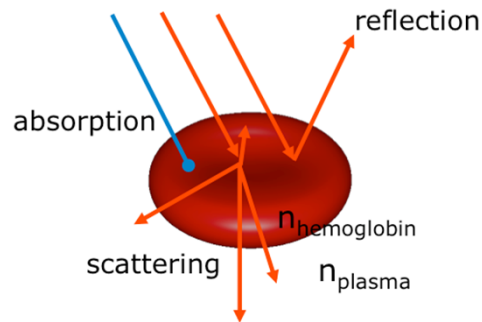
Relatively cheap (~\$3 for TiO₂)

Liquid phantoms?



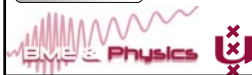
Interaction: light-RBC

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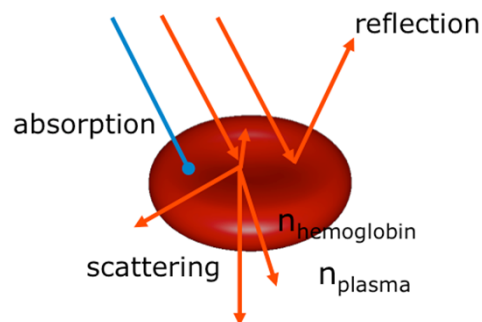
effects of scattering with concentration?

$$\mu_s = \sigma_s \cdot \leftarrow$$



Interaction: light-RBC

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non linear effects of scattering with concentration

$$\mu_s \neq \sigma_s \cdot \leftarrow \text{above 1 vol\%}$$

$$\text{For whole blood: } \mu_{S,blood} = (1 - hct)^2 \frac{hct}{V_{RBC}} \sigma_{S,RBC}$$

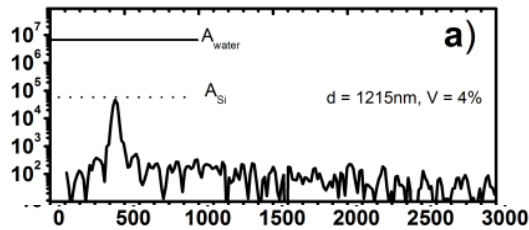
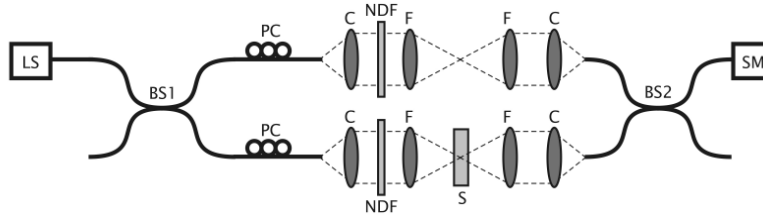


Bosschaart et al Lasers Med Sc 2014

μ_s for high concentrations?

- transmission OCT measurements

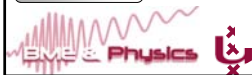
(1300 nm spectral domain home built system, coherence length 12 μm)



Optical Path Length (μm)

Nguyen et al Optics Express 2013

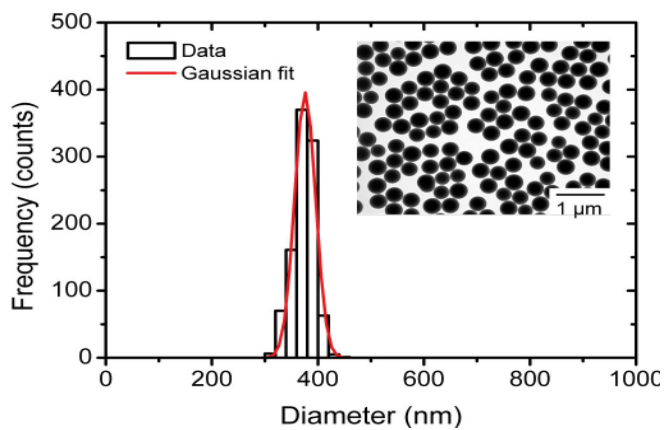
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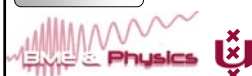
μ_s for high concentrations

Silica beads (0.5, 0.8, 1.0 and 1.5 μm)

Size distribution by EM measurements



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Nguyen et al Optics Express 2013

μ_s for high concentrations

Silica beads

Mie calculations (1300 nm, silica, $n=1.447$ in water, $n=1.32$)

introduction

OCT signal

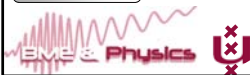
Phantoms:

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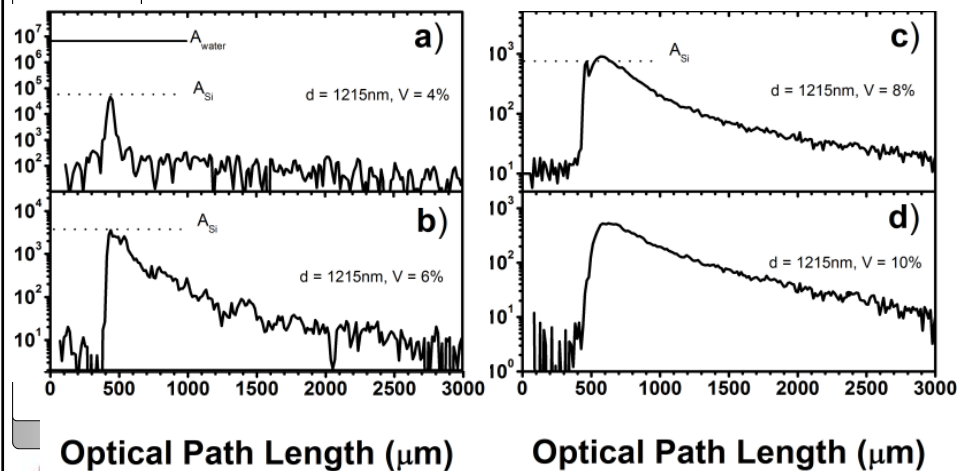
Cat. #	Diameter (SD) (nm)	Scattering Cross section (μm^2)	Anisotropy factor	Max. Vol. (%)
Psi-0.5	376 (20)	0.0012451	0.253	20
Psi-0.8	759 (14)	0.031297	0.742	20
Psi-1.0	906 (17)	0.069361	0.781	10
Psi-1.5	1215 (18)	0.24026	0.869	10



Nguyen et al Optics Express 2013

μ_s for high concentrations

Transmission results for 1215 nm silica beads at 4, 6, 8 and 10 vol%

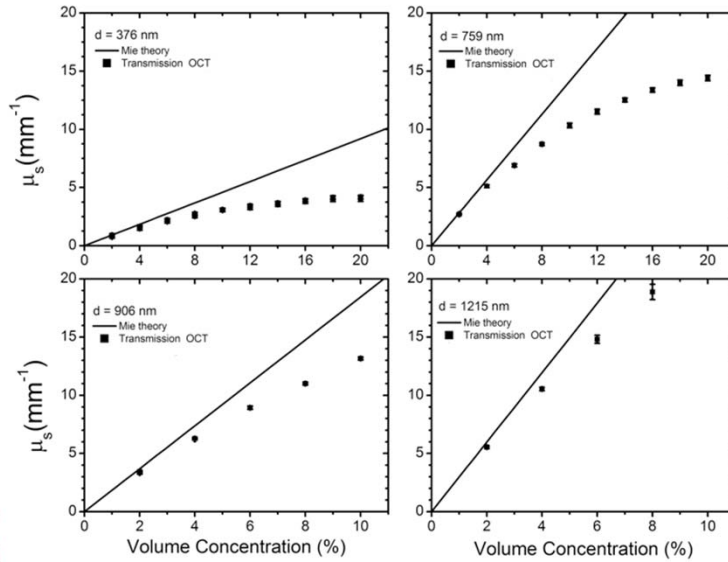


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μ_s for high concentrations

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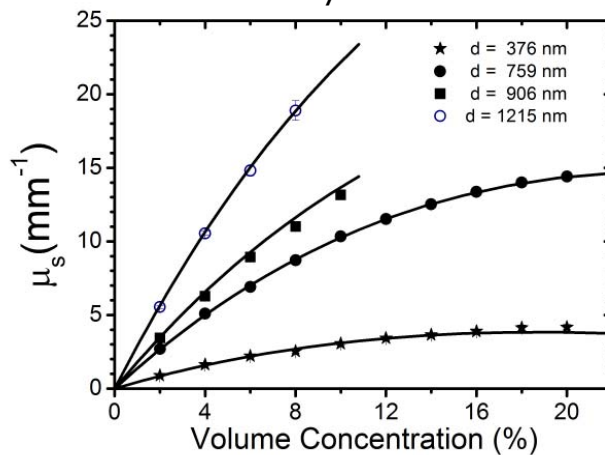
• Transmission results for all beads



μ_s for high concentrations

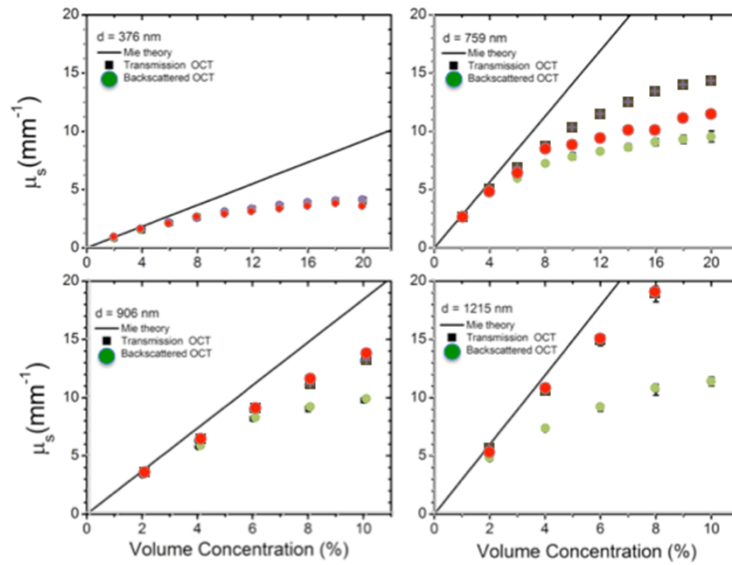
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Dependent scattering for all beads
 Corrected for dependent scattering with structure factor by Percus-Yevick model



OCT: multiple versus dependent scattering

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 - silicone
 - [liquid](#)
- conclusion

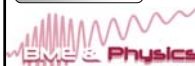
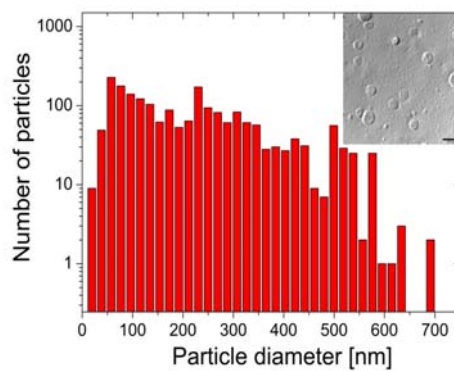


● EHF results: Under restricting conditions for θ_{RMS} (g)

Dependent scattering for IL

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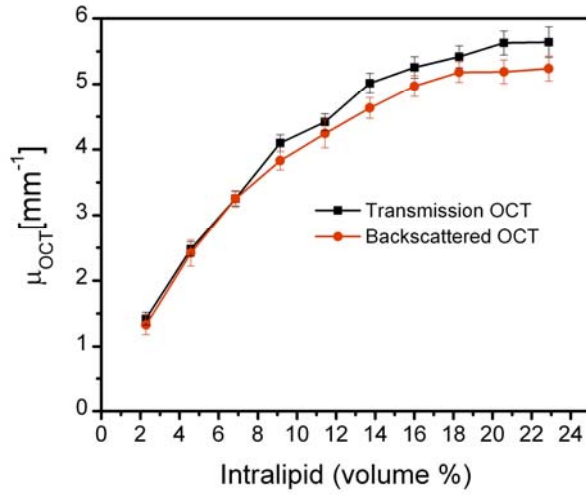
How about Intralipid?



Kodach et al. Optics Express, 2011, Vol. 19, pp. 6131-6140

Dependent scattering for IL

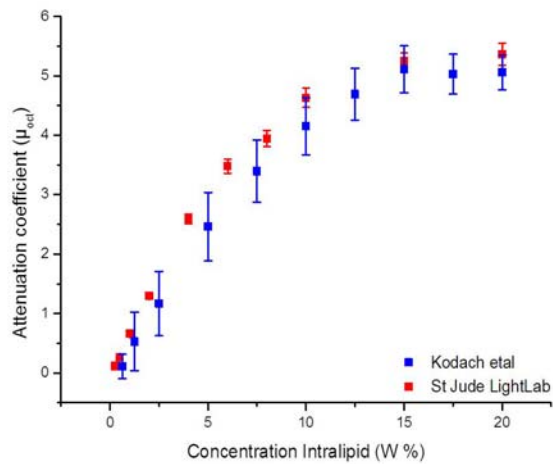
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Different OCT systems

After probe calibration, @ 1300 nm: maximal attenuation in IL is $\sim 5 \text{ mm}^{-1}$

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Kodach et al. Optics Express, 2011, Vol. 19, pp. 6131-6140

Conclusions: scattering measured by OCT

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liquid

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OCT signal analysis give insight in fundamental and in vivo scattering properties

- Stable tissue mimicking phantoms
- Dependent scattering (> 1 vol%)
- Attenuation determination *in vivo*

$$i_{\text{det}}(z) = \eta \text{Re} \left\{ \gamma \left(\frac{2zn_{\text{med}}}{c} \right) \right\} \otimes h(r, z) \sqrt{P_{\text{ref}} P_{\text{sample}}} \sqrt{\mu_{b,NA}} \sqrt{\exp(-2\mu_s z)}$$

- How is the signal processed?
- Lateral resolution?

